

Cellulose hydrogels physically crosslinked by glycine: Synthesis, characterization, thermal and mechanical properties

S. Palantöken ¹, K. Bethke ¹, V. Zivanovic ¹, G. Kalinka ², Janina Kneipp ¹, Klaus Rademann ¹

¹Institut für Chemie, Brook-Taylor Str. 2, Humboldt Universität zu Berlin, 12489, Berlin, Germany

²BAM, 5.3, Unter den Eichen 87, 12205, Berlin, Germany

Correspondence to: S. Palantöken (E-mail: sinem.palantoeken@chemie.hu-berlin.de)

ABSTRACT: Biopolymers are very efficient for significant applications ranging from tissue engineering, biological devices to water purification. There is a tremendous potential value of cellulose because of its being the most abundant biopolymer on earth, swellability, and functional groups to be modified. A novel, highly efficient route for the fabrication of mechanically stable and natural hydrogels is described in which cellulose and glycine are dissolved in an alkaline solution of NaOH and neutralized in an acidic solution. The dissolving temperature and the glycine amount are essential parameters for the self-assembly of cellulose chains and for tuning the morphology and the aggregate structures of the resulting hydrogels. Glycine plays the role of a physical crosslinker based on the information obtained from FTIR and Raman spectra. Among the prepared set of hydrogels, CL5Gly30 hydrogels have the highest capacity to absorb water. The prepared CL5Gly30 gels can absorb up to seven times their dry weight due to its porous 3-D network structure. CL5Gly10 hydrogel exhibits 80% deformation under 21 N force executed. The method developed in this article can contribute to the application of heavy metal adsorption in aqueous solutions for water purification and waste management. © 2019 The Authors. *Journal of Applied Polymer Science* published by Wiley Periodicals, Inc. *J. Appl. Polym. Sci.* **2019**, 136, 48380.

KEYWORDS: biopolymer; cellulose; hydrogel; natural; synthesis

Received 5 April 2019; accepted 17 July 2019

DOI: [10.1002/app.48380](https://doi.org/10.1002/app.48380)

INTRODUCTION

Hydrogels are three-dimensional hydrophilic network structures provided via irradiation,¹ chemical or physical crosslinks in the macromolecular chains.^{2,3} Over the past decades, there has been a dramatic increase in the number of biopolymer hydrogel fabrications due to their unique properties such as swellability, nontoxicity, biodegradability, and biocompatibility.^{4–8} As it is also addressed in Water, Waste and Energy Management 2018 and Green Chemistry and Sustainability Engineering 2018 conferences*; hydrogels are attracting widespread interest in fields of personal hygiene products,⁹ underwater devices,¹⁰ water reservoirs for dry soils,^{11,12} soft contact lenses,¹³ water purification,^{14,15} surface coatings,¹⁶ controlled drug release systems,^{2,17} tissue engineering, wound healing dressings,¹⁸ and cell immobilization^{19,20} regarding their biocompatibility and biodegradability.²¹

Cellulose is the polymer of glucose, and it is found in copious amounts in plants and natural fibers²² [Figure 1(a)]. It is

environmentally friendly and leaves little traces of carbon footprint. It is classified as bacterial cellulose (BC) or plant cellulose (PC) according to its sources. The glucose units are held together by 1,4- β -glycosidic linkages. BC has more benefits compared to PC. It has an ultrafine fiber network structure and better mechanical properties. Additionally, BC is obtained purely, while PC is associated with lignin and pectin. Because of its lignin content, the PC requires further purification steps.²¹ In this study, microcrystalline cellulose from *S3 Handel und Dienstleistungen UG* (CAS. 9004-34-4) is used.

Particular attention has been paid to develop cellulose-based devices for biomedical applications, biosensors,²³ supercapacitors,²⁴ and nanocomposite hydrogels.²⁵ It is important to emphasize that cellulose is a bio-durable material. Since animal and human tissues are not able to synthesize *cellulase* enzymes, resorption of cellulose does

Additional Supporting Information may be found in the online version of this article.

© 2019 The Authors. *Journal of Applied Polymer Science* published by Wiley Periodicals, Inc.

This is an open access article under the terms of the Creative Commons Attribution License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited.

*Water, Waste and Energy Management 2018, 18–20th July 2018, Madrid, Spain, <http://waterwaste18.com/>. Green Chemistry and Sustainability Engineering 2018, 23–25th July 2018, Madrid, Spain, <http://greenchemistry18.com/>.

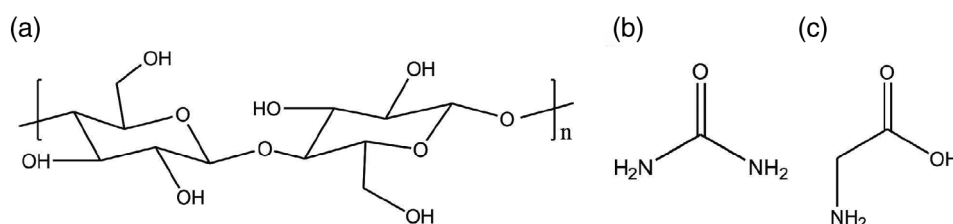


Figure 1. Molecular structure of cellulose (a), urea, (b) and glycine (c). [Color figure can be viewed at wileyonlinelibrary.com]

not occur.²¹ This feature of cellulose has triggered the development of flexible cellulose compositions for the use of artificial nerves in 3D printed electronic structures.²⁶

A high number of crosslinking agents and catalysts have been studied to produce cellulose derivative hydrogels. As crosslinkers in cellulose hydrogels mostly epichlorohydrin,^{27,28} aldehydes,²⁹ urea derivatives,³⁰ carbodiimides³¹ and carboxylic acids^{32,33} are used.²¹

During the dissolution of cellulose in sodium hydroxide solutions at lower temperatures, the gelation process occurs owing to the cellulose–cellulose network formation associated with a micro-phase separation of urea [Figure 1(b)].³⁴ However, the role of urea in cellulose dissolution is not understood very well. There are two $-\text{NH}_2$ groups joined by a carbonyl ($\text{C}=\text{O}$) functional group in the molecular structure of urea.

Glycine is the simplest amino acid, which has a primary amine and a carboxylic acid group [Figure 1(c)]. Fabrication of cellulose hydrogels via crosslinking them with glycine has been a question of great interest.³⁴ As glycine is amphoteric, it would be a practical candidate to work in acidic and basic solutions.

Yao *et al.* have investigated crosslinking of cotton cellulose in the presence of serine, glycine, and dimethyloldihydroxyethyleneurea and the physical properties of the crosslinked fabrics.³⁵ Remadevi *et al.* described glycine-treated cotton fibers at different pH values and studied their tensile, physical, and microstructure

properties.³⁶ However, hydrogel preparation with crosslinking of microcrystalline cellulose by glycine has not been at the primary focus of any research groups to the best of our knowledge. The idea of self-assembled cellulose-glycine hydrogels has also not been covered by the literature.

In this work, our goal is preparing cellulose hydrogels with glycine in alkaline medium. The swelling behavior, bonding structure, morphology, reusability, thermal and mechanical properties were systematically investigated at different glycine amounts. It was found that the hydrogel CL5Gly30 (Alkaline glycine solution amount is 30% [v/v] of the total volume) demonstrated a high swelling degree due to its highly porous structure. In addition, mechanical strength was much higher at CL5Gly10 (glycine amount is 10% [v/v]) than neat cellulose in 80% deformation. As seen from the results, CL5Gly30 seems to be a potential substrate for heavy metal ion adsorption in the case of an adsorptive agent being loaded in the hydrogels.

EXPERIMENTAL

Materials

Cellulose powder was purchased from S3 chemicals and was used without further purification, and it was always kept in the oven at 55 °C to get rid of the humidity in the material. The molecular weight is 324.28 g mol^{-1} and degree of polymerization is below 350. Glycine was purchased from Alfa Aesar, Kandel-Germany.

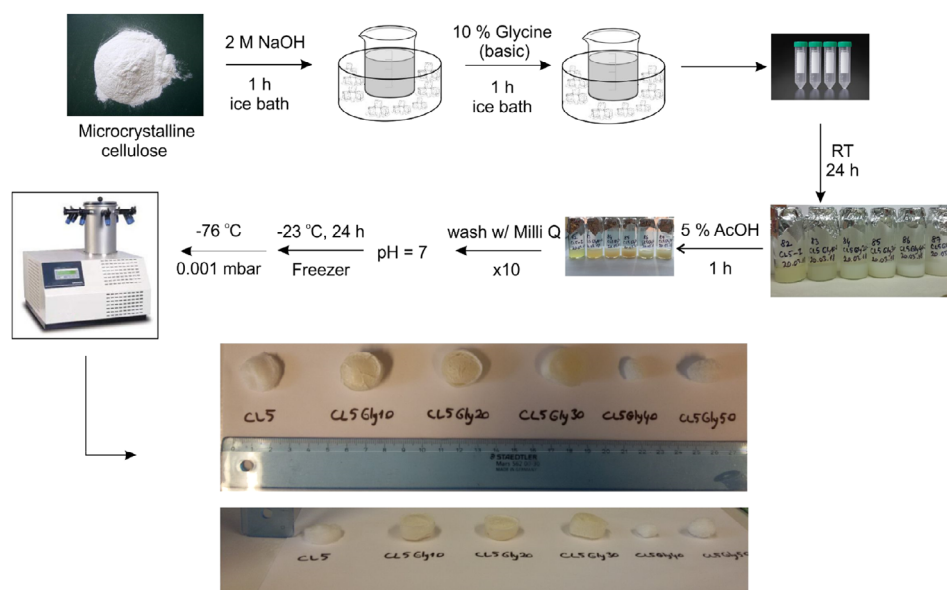


Figure 2. Experimental procedure for preparing cellulose and cellulose–glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

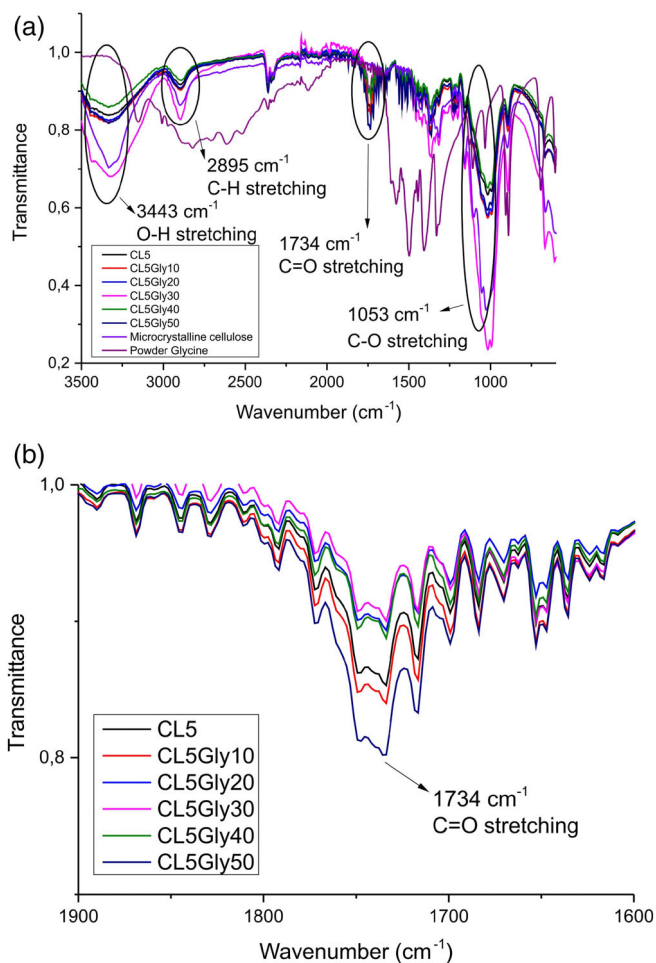


Figure 3. Fourier transform infrared spectra of cellulose hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

Ultrapure water (Milli-Q) was used to prepare the aqueous solutions of 2 M NaOH and 5% acetic acid.

Synthesis of Pure Cellulose and Cellulose-Glycine Hydrogels

An amount of 0.5 g of cellulose was dissolved in 10 mL of NaOH (2 M) and mixed in an ice bath (0–4 °C) for 1 h vigorously. CL5 denotes the cellulose amount that is dissolved in NaOH (0.5 g of cellulose). Additionally, an alkaline solution of glycine (10% w/v) is prepared by dissolving glycine in 2 M NaOH to use in the further steps. Different kinds of hydrogels were prepared. These CL5 hydrogels do not have glycine in it. CL5Gly10, CL5Gly20, CL5Gly30, CL5Gly40, and CL5Gly50 contain glycine with 10, 20, 30, 40, and 50 vol % of the total volume NaOH solution, respectively. For the glycine containing hydrogels, cellulose is dissolved in NaOH initially for 1 h. Successively, the calculated amount of glycine solution is added, and the mixture was stirred for an additional 1 h in the ice bath. After an additional hour of mixing, the viscous solution of cellulose is poured into molds and left overnight at room temperature. The following day, the gels were washed with 5% acetic acid (1 h) for neutralization. Additionally, the samples are washed several times until the pH of 7 is reached. Subsequently, the hydrogels were frozen at –23 °C and then

lyophilized at –76 °C at 0.001 mbar (Alpha 1-4 LDPlus Freeze-Dry, Christ) (Figure 2).

Characterization Methods

The swelling behavior of the hydrogels was studied by gravimetric measurements. The freeze-dried hydrogels were weighed and immersed in Milli-Q water, and subsequently, time-dependent analysis of the swollen hydrogels was conducted. Samples are removed from the water and reweighed to study the time-dependent water uptake. All measurements took place at 25 °C in a water bath. The percent swelling was calculated with the following equation:

$$S\% = (m_t - m_0) / m_0 \times 100, \quad (1)$$

where m_t is the mass of the swollen gel at time t and m_0 is the mass of the dry gel.

The mechanical tests for the wet strength of the hydrogels were conducted with a modified Adamel Lhomargy DY.20B compression test apparatus. As the transducer, a high sensitive piezo electric force sensor Kistler 9311B was used and it was operated by a charge amplifier type Kistler 5011. The velocity of the traveling head was closed loop controlled by software developed in Bundesanstalt für Materialforschung und–prüfung (BAM). The software was also used for recording the time, force, and

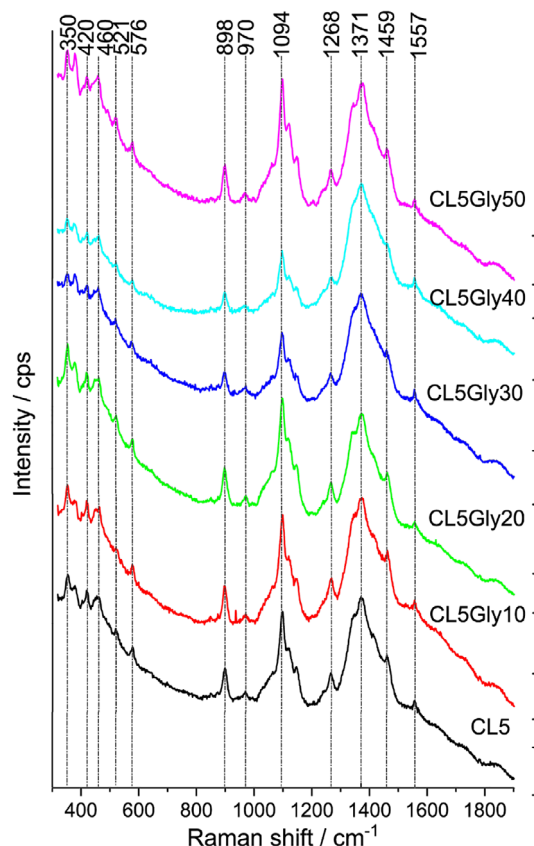


Figure 4. Raman spectrum of cellulose and cellulose–glycine hydrogels. Excitation wavelength, 785 nm; laser intensity, $1.4 \times 10^6 \text{ W cm}^{-2}$; acquisition time, 5 s; scale bars: 100 cps. [Color figure can be viewed at wileyonlinelibrary.com]

Table I. Summary of Observed Raman Frequencies and Band Assignments of Cellulose–Glycine Hydrogels, Based on Refs. 38–40

Raman shift (cm ⁻¹)	Tentative band assignment
350	CCC, COC, OCC, OCO skeletal bending, CCH, COH methane bending, movement of CC, CO groups within the ring units
420	
460	
521	
576	
898	HCC, HCO bending, NH ₂ twist
970	HCH bending
1094	COC stretching symmetric
1268	HCH (wagging), HCC, HOC, COH (rocking) bending, CH ₂ twist
1371	
1459	HCH scissoring
1557	bending

displacement during the test. The maximum speed of the traveling head was 1 mm s⁻¹. However, the pressure tests with a velocity of 0.2 mm s⁻¹ were used. The force range was in 50 N in pressure mode and the force sensor was calibrated by using a reference weight of 2 kg to match the force arising in the pressure tests.

Attenuated total reflection Fourier transform infrared spectra were collected in a Bruker VERTEX 70v FTIR spectrometer equipped with a DLa-TGS detector, using a diamond prism.

Raman spectra were excited at a laser wavelength of 785 nm with an excitation intensity of 1.4×10^6 W cm⁻² provided by a continuous-wave diode laser. The sample was placed on a CaF₂

slide and the excitation light was focused on the specimens through a microscope objective. Raman spectra were acquired for durations of 1–5 s, depending on the sample. The Raman light was collected in backscattering geometry and detected by liquid nitrogen-cooled CCD (Horiba, Munich, Germany). The Raman spectra were frequency calibrated using a spectrum of toluene–acetonitrile (1:1) mixture.

Thermal gravimetric analysis (TGA) measurements were performed on a PerkinElmer Pyris 1 TGA.

RESULTS AND DISCUSSION

Fabrication of Cellulose–Glycine Hydrogels

FTIR spectra were obtained from the samples CL5, CL5Gly10, CL5Gly20, CL5Gly30, CL5Gly40, and CL5Gly50. All of these hydrogels show characteristic vibrational bands of cellulose bands, such as the O–H, CH, and C–O stretching vibrations at 3443, 2895, and 1053 cm⁻¹, respectively, in accordance with literature.³⁷ (Figure 3) Glycine is believed to function as a physical crosslinker as the carbonyl stretching at 1734 cm⁻¹ does not have a distinct shift in the spectrum. Similarly, the absence of an amide or an ester band at around 1680 cm⁻¹ is an indication that the chemical crosslinking between cellulose chains and glycine does not occur.³⁸ (Figure 3).

In the samples CL5Gly60, CL5Gly70, CL5Gly80, CL5Gly90, and CL5Gly100, no gelation was observed. Here, Raman spectroscopy was used to find out about possible covalent bonding with glycine by observing the frequencies of characteristic cellulose vibrational bands.

The Raman spectra of cellulose and the cellulose–glycine hydrogels are shown in Figure 4 for the 300–1900 cm⁻¹ spectral range. Due to the overlapping bands assignments of glycine and cellulose, it is challenging to observe a very clear broadening or shifting of the band

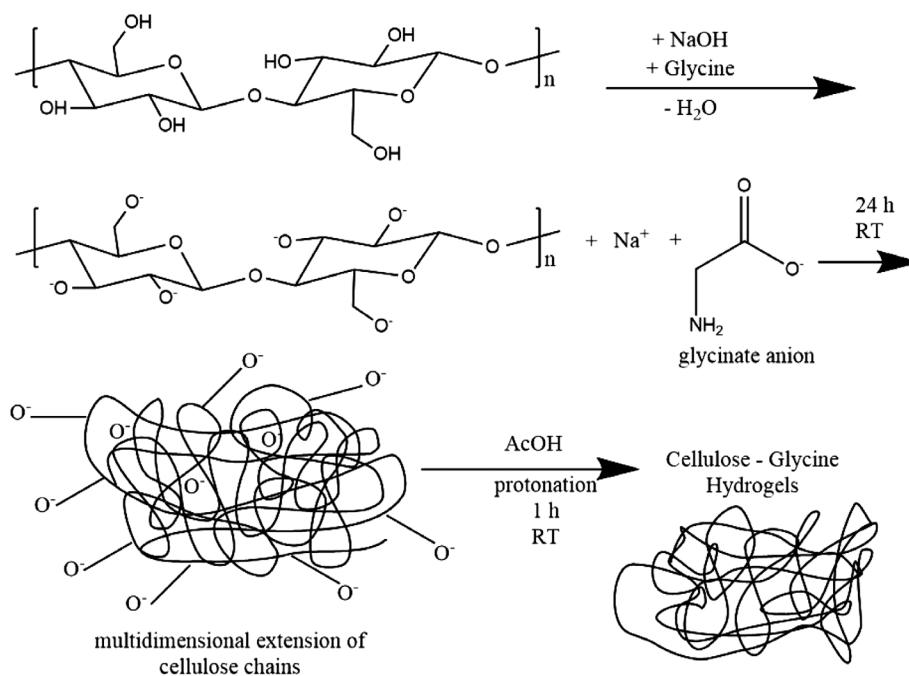


Figure 5. Scheme for physical crosslinking of cellulose hydrogels with glycine. [Color figure can be viewed at wileyonlinelibrary.com]

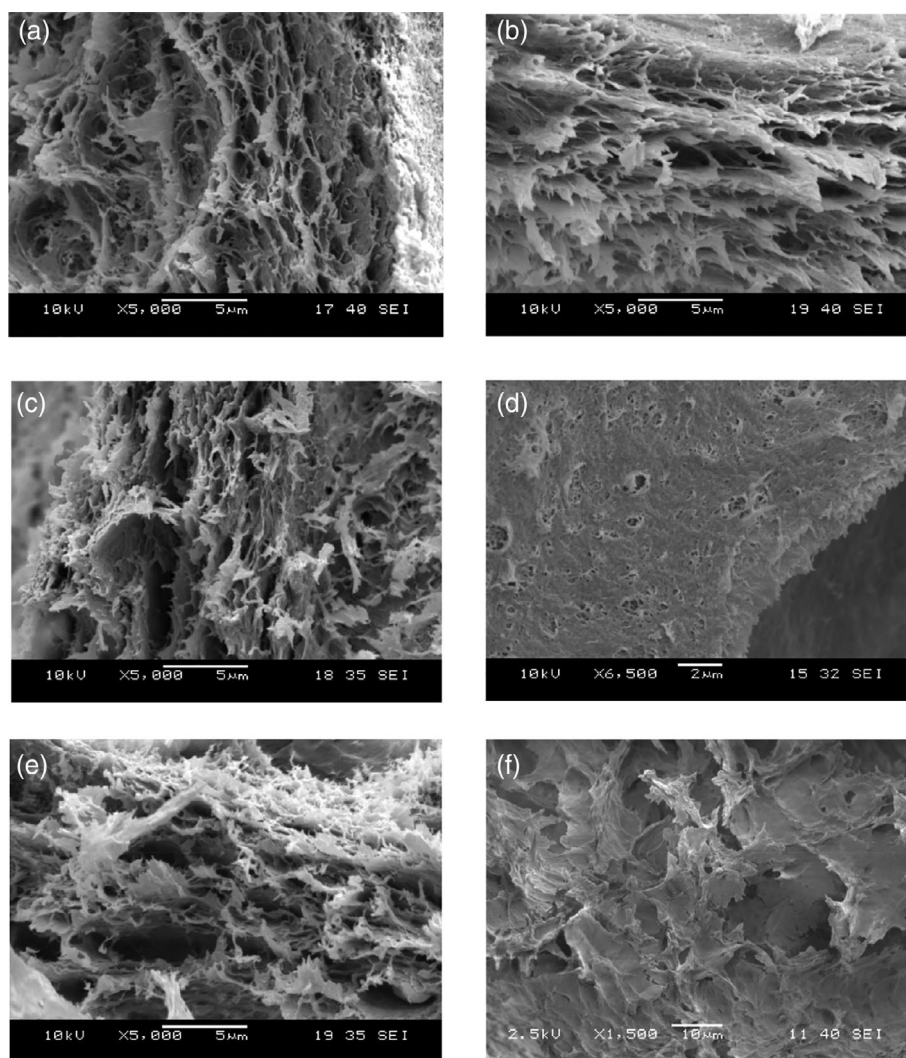


Figure 6. SEM images of cellulose hydrogels with different compositions of glycine (a) CL5 ($\times 5000$ magnification), (b) CL5Gly10 ($\times 5000$), (c) CL5Gly20 ($\times 5000$), (d) CL5Gly30 ($\times 6500$), (e) CL5Gly40 ($\times 5000$), (f) CL5Gly50 ($\times 1500$) hydrogels (Jeol, JSM – 6060 with the imaging software of SEM Control User Interface V6.55 by JEOL). [Color figure can be viewed at wileyonlinelibrary.com]

frequencies, since the changes are expected to be relatively small. As it can also be seen in Table I, all spectra display bands assigned to cellulose vibrations, in accordance with previously published data.^{39,40} The sharp COC symmetric stretching mode at 1095 cm^{-1} and HCC, HOC, and COH bending vibrations at 1371 cm^{-1} for cellulose are visible. In glycine containing hydrogels, the peak due to NH_2 twisting mode (898 cm^{-1}) and CH_2 twisting mode (1372 cm^{-1}) shows a slight increase in intensity. The intensity change could be due to the increase in the amount of glycine in the cellulose hydrogels.³⁸ The intensity increase of the skeletal bending and the movement of the carbon groups within the ring units between $350\text{--}576\text{ cm}^{-1}$ could be due to the interactions between glycine and cellulose. Significant findings of FTIR and Raman spectra are that the crosslinking between the cellulose and the glycine is very likely physical rather than chemical.

Crosslinking in polymer chemistry leads to a multidimensional extension of polymeric chains which results as a network structure. It can be classified as ionic (physical) or covalent (chemical).

When a polymer is in liquid form, it can turn into a “solid” or “gel” due to the chain crosslinking. Great attention is paid to crosslinked polymers as they are relatively resistant to heat, wear, and solvents in addition to being mechanically strong.⁴¹

Crosslinkers are generally known as toxic and physically crosslinked hydrogels are considered innovative because of being an alternate solution for crosslinker toxicity. Physically crosslinked hydrogels can be formed by hydrogen bonds, crystallization, ionic interactions, protein interaction or from amphiphilic graft and block polymers.⁴² In this case, it results from hydrogen bonding because the protonation of the carboxylic acid group in glycine takes place and pH-dependent swelling of the gels occurs. Ionic interactions are also important because cellulose is dissolved in NaOH (2 M) in an ice bath for the extension of cellulose chains to form a multidimensional structure (Figure 5).⁴²

Qualitative gravimetric analysis is also conducted in order to reveal the actual amount of glycine that incorporated in the hydrogel. Ninhydrine test is conducted for this aspect. Ninhydrine test is a

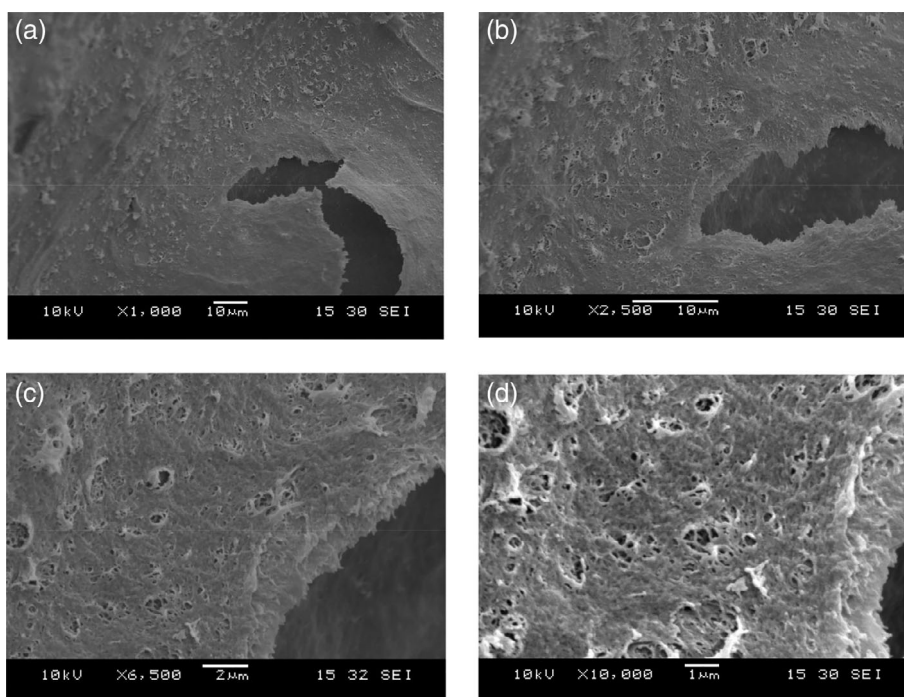


Figure 7. Different magnification SEM images of CL5Gly30 hydrogels (a) $\times 1000$, (b) $\times 2500$, (c) $\times 5000$, (d) $\times 10\,000$ (Jeol, JSM – 6060 with the imaging software of SEM Control User Interface V6.55 by JEOL). [Color figure can be viewed at wileyonlinelibrary.com]

sensitive test for primary amines to produce an intense blue color. Only CL5Gly50 gave a slightly blue color. It can be considered that ninhydrine reacts with the deprotected amine groups of the free glycine remained in the hydrogel; however, one must be really careful to claim it as there is no distinct shift observed in FTIR and Raman spectra of cellulose–glycine hydrogels.

Morphology and Water Absorption Capacity of Cellulose–Glycine Hydrogels

Scanning electron microscope (SEM) was used to analyze the surface morphology and microstructure of cellulose hydrogels. As can be

seen in Figures 6 and 7, the cellulose–glycine hydrogels have three-dimensional network structure where the pores are evenly distributed. Micro-roughness of the hydrogels can be a benefit for the tissue engineering application as cellular adhesion, proliferation, and tissue formation are required for the scaffolds.⁴³

The swelling curve of neat cellulose hydrogel and the hydrogels with different amounts of glycine are monitored conducting the test for three times for each sample, and the curves are drawn by taking the average values of the data for each point. The graph is shown in Figure 8 in accordance with the standard deviation for each curve. Standard deviation for each curve can be seen in detail in Figures S1,

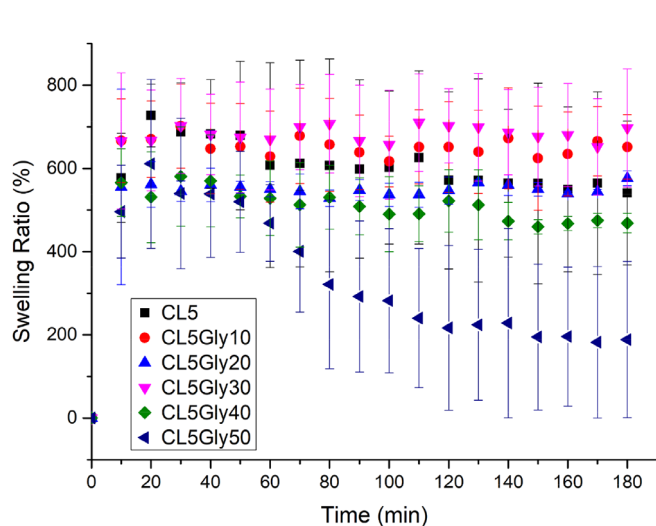


Figure 8. Swelling curves for cellulose and cellulose–glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

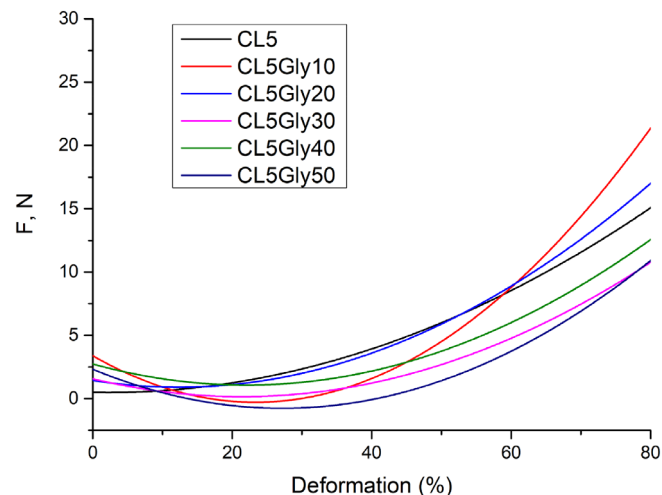


Figure 9. Polynomial fitting of compressive force–deformation curves for cellulose and cellulose–glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

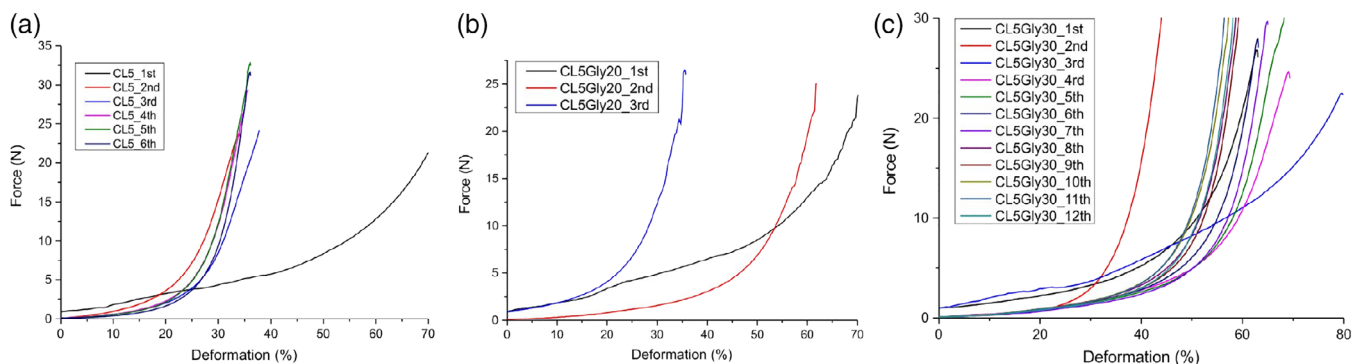


Figure 10. Compressive force–deformation curves for repetitive tests of (a) CL5, (b) CL5Gly209 and (c) CL5Gly30 hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

S2, S3, S4, S5, S6. Swelling increases with time up to a certain level and then it reaches an equilibrium state between swelling and deswelling. The equilibrated swollen state is reached in 1 h for CL5Gly10, CL5Gly20, CL5Gly30, and CL5Gly40. The water absorption decreases for the hydrogels CL5 and CL5Gly50 due to the separation of the hydrogels into smaller pieces.

The first quantities of water being absorbed by a gel might originate from the microvoids considering that capillary forces retain water. As CL5Gly30, hydrogel composition shows the optimum swelling behavior among cellulose hydrogels, it has been accepted the optimum 3-D network structure, which also can be observed in SEM images. Swelling capacity was improved from 600 to 700% (Figure 8).

Mechanical Properties of Cellulose–Glycine Hydrogels

There are various methods to study the mechanical properties of hydrogels. A dumbbell shape is used for most uniaxial tensile testing. However, for self-assembly material presented here, it is not possible to shape them before testing as they can get distorted. Therefore, uniaxial compression is more suitable for cellulose–glycine hydrogels as they are examined in the swollen state. The mechanical properties of cellulose and cellulose–glycine hydrogels under uniaxial compression have been studied at ambient

temperature in the swollen state. The output of the mechanical tests was given as polynomial fitting of force (N) versus deformation (%) curves of cellulose and cellulose hydrogels. A minimum number of five measurements were conducted for each composition and average multiple curves for each composition were sketched and the polynomial fits were compared (Figure 9).

The force versus deformation curves differ at initial and higher rates of compression for the same sample as the sample geometry was not uniform at the beginning of the test. The geometry of the swollen network becomes more uniform at the higher rate of compression. Owing to that, the stiffness at higher compression rates is easier to compare than the beginning of the test (Figure 9).

As expected, that the hydrogen bonds in the hydrogel structure act as crosslinks and the microcrystalline structure of cellulose shorten the elastic behavior of chains and the chain motion is restricted.⁴⁴ Hydrogen bonds have a nonpermanent character and it leads to the spontaneous association of network junctions. Highly swollen CL5Gly10 and CL5Gly20 hydrogels exhibit rubbery networks and the correlation that higher force is needed for the same amount of deformation was previously interpreted. CL5Gly10 hydrogel exhibits 80% deformation under 21 N force executed. It is almost 1.5-fold of

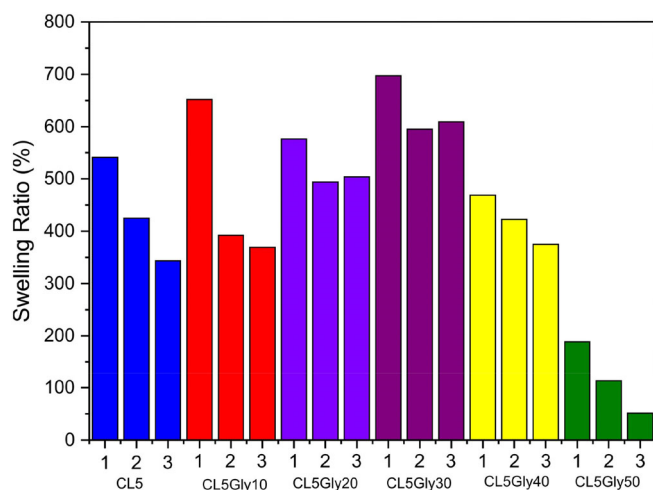


Figure 11. Swelling ratio for repetitive tests of cellulose and cellulose–glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

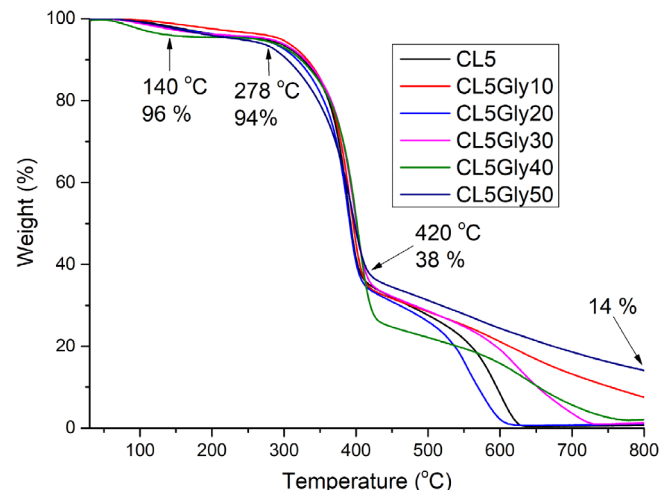


Figure 12. TGA thermograms of cellulose and cellulose–glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

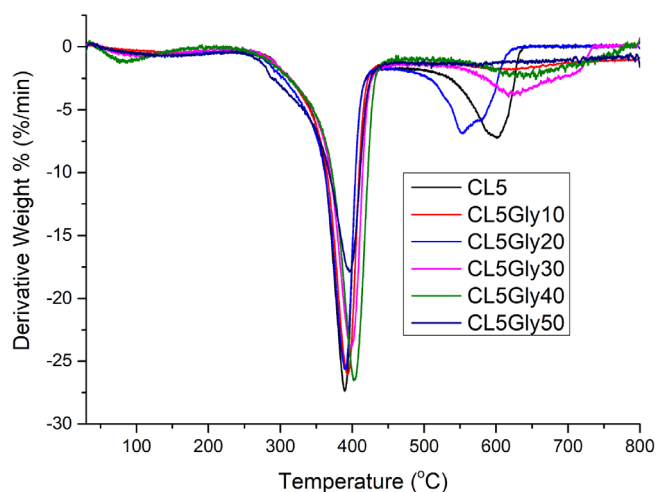


Figure 13. TGA derivative thermograms of cellulose and cellulose-glycine hydrogels. [Color figure can be viewed at wileyonlinelibrary.com]

the force, which is needed to deform the same percentage of the cellulose hydrogels without glycine. For the cellulose-glycine hydrogels with the lowest water content (CL5Gly40—450%, CL5Gly40—200%), distortion increases drastically even if a small amount of force is exerted. It is probable that cellulose-glycine hydrogels behave as crosslinked when sufficiently swollen.

Reusability of Cellulose-Glycine Hydrogels

Particular attention is paid to the reusability of the hydrogels. The force is exerted repetitively to observe the response of the hydrogels. It is noticed that an increased amount of force is required in the repeated cycles to result with the same amount of deformation [Figure 10(a-c)]. It can be explained with the microvoids disappearing with the force, which has already been exerted in the initial trial. When these hydrogels are tested

multiple times in a row, they are subject to water loss during the compression.⁴⁵ Microcrystalline cellulose hydrogels are brittle and when the water is squeezed out, no more recovery can be observed in swelling. It is probable to conclude that the network structure in cellulose-glycine hydrogels is diminished and they are broken into fragments.

When there is no force exerted on the hydrogels and repetitive swelling experiments are conducted with the initial sample for each composition, a decrease in the swelling ratio is observed (Figure 11). However, a similar trend in the order of swelling ratio for the hydrogels is kept.

Thermal Properties of Cellulose-Glycine Hydrogels

Thermal gravimetry (TG) measurements were done in the temperature range from 30 to 800 °C with a heating rate of 20 °C min⁻¹. The temperature range is kept wide enough in order to observe the possible changes in more detail. The TG experiments were performed once for each cellulose hydrogel composition under Ar using open pans. The sample masses varied between 3 and 14 mg. Additionally, for Figure S7, TG measurements were done from 250 to 750 °C with a rate of 5 °C min⁻¹. The thermogram of CL5Gly20 and CL5Gly30 hydrogels can be seen in a rough or more detailed curve.

As cellulose has six hydrophilic groups per unit molecule, which provide the possibility for water take up. There are three types of water in hydrophilic polymers: bound (nonfreezing), freezing-bound, free (not bound). The dry hydrogel samples were heated at a rate of 20 °C min⁻¹. During the increase of temperature from 30 to 140 °C, there is a decrease in the weight of about 4% (see Figure 12), which corresponds to the loss of water from the cellulose sample. There is a small amount of water, which is firmly bonded to cellulose molecules because dehydration process occurs at temperatures higher between 140 and 280 °C. Further loss of sample masses is monitored during the heating runs. The

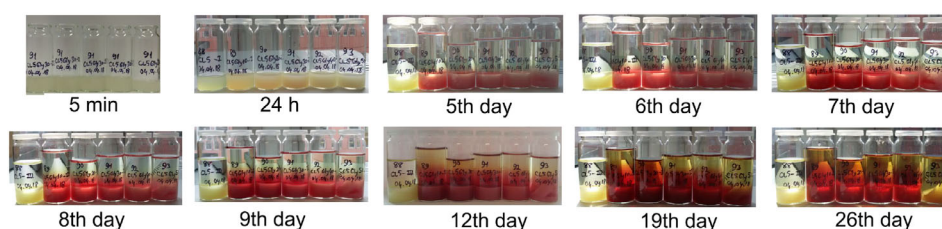


Figure 14. Photos of CL5 and CL5Gly10–50 hydrogels that are kept in pH 13. [Color figure can be viewed at wileyonlinelibrary.com]

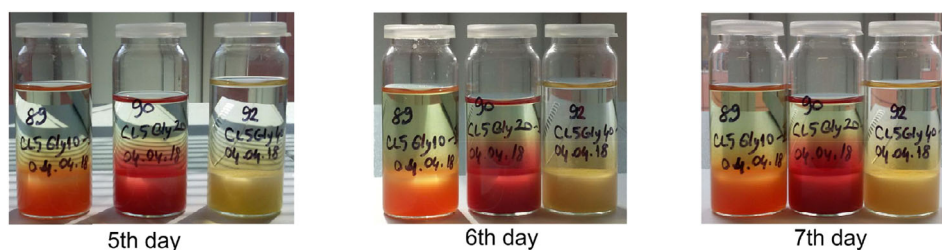


Figure 15. Photos of CL5Gly10, CL5Gly20, and CL5Gly40 hydrogels that are kept in different solvents. [Color figure can be viewed at wileyonlinelibrary.com]

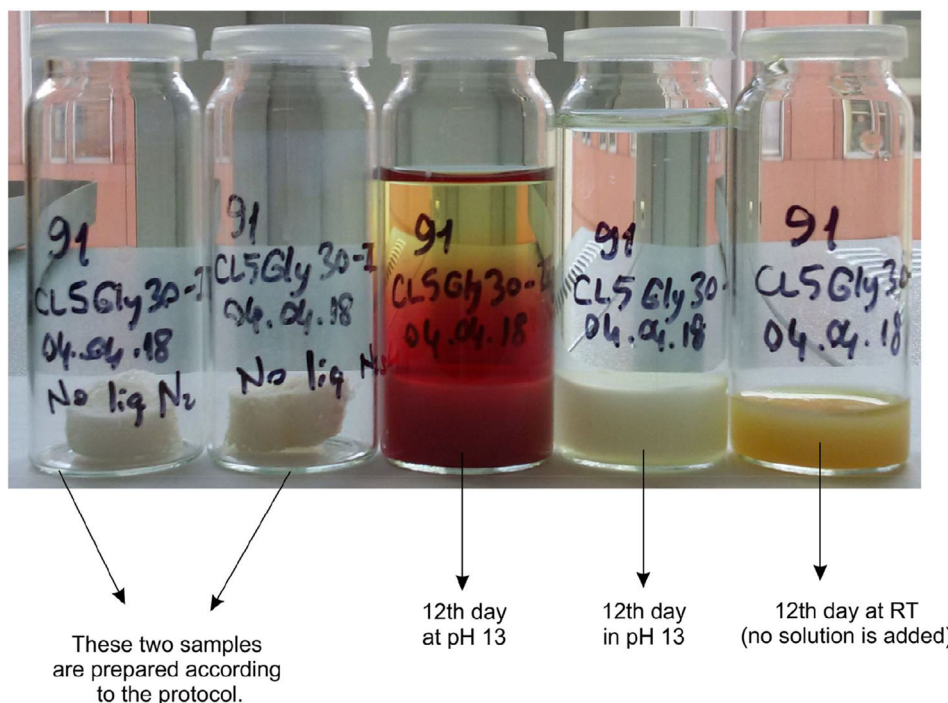


Figure 16. Photos of CL5Gly30 after different treatments. [Color figure can be viewed at wileyonlinelibrary.com]

weight loss of cellulose mass observed between 278 and 420 °C reflects the thermal decomposition. There is a two-step process for some of the samples, and it can be seen easily in derivative thermograms (Figure 13). The second step of decomposition takes place between 420 and 600 °C. These curves show that the hydrogels are not durable above 280 °C, which is in good agreement with the previous studies on cellulose.⁴⁶

Pink/Red Color of Cellulose–Glycine Hydrogels at Alkaline Condition

An orange–pink–red color of transition is observed when the hydrogels are kept in highly alkaline solutions. Samples that are shown in Figures 14, 15, and 16 are the examples of this observation.

The red color was observed in every composition of cellulose–glycine hydrogels except neat cellulose hydrogels. It is reasonable to suppose that those red pigments are the by-products of a D-Xylose–glycine reaction system. Shirahashi *et al.* studied a similar D-Xylose–glycine reaction system indicating red pigments as important Maillard reaction intermediates.⁴⁷

The hydrogels in Figure 16 (CL5Gly30) were prepared in the same beaker and they have the same experimental parameters. After the polymerization, first and second vials are treated the way explained in the experimental part and dry hydrogels are obtained. The third one was kept in water and has the pH of 13 due to the release of NaOH from the biopolymer. The fourth one in the row was kept in NaOH for 1 h and after extensive washing with water, by-products causing the red color were removed. It was washed until pH of 7 was obtained. Afterward, the vial was again filled with NaOH (2 M) in order to obtain the possible color change to red, but it was not observed. The fifth

sample was kept at room temperature as a reference to see the changes and compare it with the others. Comparing with the initial image of CL5Gly30 sample, it can be said that it turns into more yellow.

CONCLUSIONS

The synthesis of cellulose hydrogels physically crosslinked by glycine is conducted straightforwardly and is easily achieved. The results are highly reproducible on average but have a small spread. All properties of hydrogels mentioned in this article, in particular swelling, porosity, mechanical strength, thermodynamic durability, stability, and reusability, lead us to suggest that novel hydrogels can be applied successfully for heavy metal or dye adsorption in the area of water purification by loading special agents in them.

It is also advised that the novel cellulose–glycine hydrogels with excellent properties can be considered as a possible candidate for tissue engineering in soft electronics and cartilage tissue engineering.

ACKNOWLEDGMENTS

The authors would like to acknowledge Humboldt Universität zu Berlin for their support of this work. Funding from DFG GSC 1013 School of Analytical Sciences Adlershof (SALSA) for the authors S.P. and V.Z. is gratefully acknowledged and K.B. is most grateful for the scholarship from the International Max-Planck Research School at the Fritz Haber Institute. The authors also thank C. Erdmann and Prof. Pinna for SEM, B. Kobin and Prof. Hecht for FTIR and TGA, F. Polster and Prof. Börner for the lyophilizer regarding the use of equipments. Portions of this work

(compression tests) were carried out with the help of G. Kalinka at BAM. The support from our colleague Mete Sungur Dalgic for proofreading is also appreciated.

REFERENCES

1. Chowdhury, M. N. K.; Alam, A. K. M. M.; Dafader, N. C.; Haque, M. E.; Akhtar, F.; Ahmed, M. U.; Rashid, H.; Begum, R. *Biomed. Mater. Eng.* **2006**, *16*, 223.
2. Peppas, N. A.; Bures, P.; Leobandung, W.; Ichikawa, H. *Eur. J. Pharm. Biopharm.* **2000**, *50*(1), 27. [https://doi.org/10.1016/S0939-6411\(00\)00090-4](https://doi.org/10.1016/S0939-6411(00)00090-4).
3. Shen, X.; Shamshina, J. L.; Berton, P.; Rogers, R. D. *Green Chem.* **2016**, *18*, 53. <https://doi.org/10.1039/c5gc02396c>.
4. Peppas, B. N. A.; Hilt, J. Z.; Khademhosseini, A.; Langer, R. *Adv. Mater.* **2006**, *18*, 1345. <https://doi.org/10.1002/adma.200501612>.
5. Nakayama, B. A.; Kakugo, A.; Gong, J. P.; Osada, Y.; Takai, M.; Erata, T. *Adv. Funct. Mater.* **2004**, *14*, 1124. <https://doi.org/10.1002/adfm.200305197>.
6. Mckee, J. R.; Appel, E. A.; Seitsonen, J.; Kontturi, E.; Scherman, O. A. *Adv. Funct. Mater.* **2014**, *24*, 2706. <https://doi.org/10.1002/adfm.201303699>.
7. Luo, K.; Yang, Y.; Shao, Z. *Adv. Funct. Mater.* **2016**, *26*, 872. <https://doi.org/10.1002/adfm.201503450>.
8. Wang, C.; Fadeev, M.; Vázquez-gonzález, M.; Willner, I. *Adv. Funct. Mater.* **2018**, *28*, 1. <https://doi.org/10.1002/adfm.201803111>.
9. Pal, K.; Banthia, A. K.; Majumdar, D. K. *Des. Monomers Polym.* **2009**, *12*(3), 197. <https://doi.org/10.1163/156855509X436030>.
10. Smith, M. J.; Flowers, T. H.; Cowling, M. J.; Duncan, H. J. *J. Environ. Monit.* **2003**, *5*(2), 359. <https://doi.org/10.1039/b209822a>.
11. Bakass, M.; Mokhlisse, A.; Lallemand, M. *J. Appl. Polym. Sci.* **2002**, *83*(2), 234. <https://doi.org/10.1002/app.2239>.
12. Johnson, M. S. *J. Sci. Food Agric.* **1984**, *35*(11), 1196. <https://doi.org/10.1002/jsfa.2740351110>.
13. Xiao, A.; Xiao, A.; Dhand, C.; Leung, C. M.; Beuerman, R. W.; Ramakrishnaef, S.; Lakshminarayanan, R. *J. Mater. Chem. B.* **2018**, *6*, 2171. <https://doi.org/10.1039/c7tb03136j>.
14. Wang, G.; He, Y.; Wang, H.; Zhang, L.; Yu, Q.; Peng, S.; Wu, X.; Ren, T.; Zeng, Z.; Xue, Q. *Green Chem.* **2015**, *17*, 3093. <https://doi.org/10.1039/c5gc00025d>.
15. Palantöken, S.; Tekay, E.; Şen, S.; Nugay, T.; Nugay, N. *Polym Compos.* **2016**, *37*(9), 2770. <https://doi.org/10.1002/pc.23473>.
16. Francois, P.; Vaudaux, P.; Nurdin, N.; Mathieu, J.; Descouts, P.; Lew, P. *Biomaterials.* **1996**, *17*(7), 667.
17. Hamidi, M.; Azadi, A.; Ra, P. *Adv. Drug Deliv. Rev.* **2008**, *60*, 1638. <https://doi.org/10.1016/j.addr.2008.08.002>.
18. Balakrishnan, B.; Jayakrishnan, A.; Kumar, S. S. P.; Nandkumar, A. M. *Trends Biomater. Artif. Organs.* **2012**, *26*(3), 139. <https://doi.org/10.1016/j.biomaterials.2005.04.012>.
19. Jen, A. C.; Wake, M. C.; Mikos, A. G. *Biotechnol. Bioeng.* **1996**, *50*(4), 357. [https://doi.org/10.1002/\(SICI\)1097-0290\(19960520\)50:4<357::AID-BIT2>3.0.CO;2-K](https://doi.org/10.1002/(SICI)1097-0290(19960520)50:4<357::AID-BIT2>3.0.CO;2-K).
20. Yang, X.; Liu, G.; Peng, L.; Guo, J.; Tao, L.; Yuan, J. *Adv. Funct. Mater.* **2017**, *27*(40), 1. <https://doi.org/10.1002/adfm.201703174>.
21. Sannino, A.; Demitri, C.; Madaghiele, M. *Materials.* **2009**, *2*(2), 353. <https://doi.org/10.3390/ma2020353>.
22. Bethke, K.; Palantöken, S.; Andrei, V.; Roß, M.; Raghuwanshi, V. S.; Kettemann, F.; Greis, K.; Ingber, T. T. K.; Stückrath, J. B.; Valiyaveettil, S.; Rademann, K. *Adv. Funct. Mater.* **2018**, *28*, 1800409. <https://doi.org/10.1002/adfm.201800409>.
23. Cunha, I.; Barras, R.; Grey, P.; Gaspar, D.; Fortunato, E.; Martins, R. *Adv. Funct. Mater.* **2018**, *27*(16), 1601755. <https://doi.org/10.1002/adfm.201606755>.
24. Pérez-madrugal, M. M.; Edo, M. G.; Alemán, C. *Green Chem.* **2016**, *18*, 5930. <https://doi.org/10.1039/c6gc02086k>.
25. Nascimento, D. M.; Nunes, Y. L.; Figueirêdo, M. C. B.; de Azeredo, H. M. C.; Aouada, F. A.; Feitosa, J. P. A.; Rosa, M. F.; Dufresne, A. *Green Chem.* **2018**, *20*, 2428. <https://doi.org/10.1039/c8gc00205c>.
26. Zhou, Y.; Wan, C.; Yang, Y.; Yang, H.; Wang, S.; Dai, Z. *Adv. Funct. Mater.* **2019**, *29*, 1. <https://doi.org/10.1002/adfm.201806220>.
27. Zhou, J.; Chang, C.; Zhang, R.; Zhang, L. *Macromol. Biosci.* **2007**, *7*(6), 804. <https://doi.org/10.1002/mabi.200700007>.
28. Zhao, D.; Huang, J.; Zhong, Y.; Li, K.; Zhang, L.; Cai, J. *Adv. Funct. Mater.* **2016**, *26*, 6279. <https://doi.org/10.1002/adfm.201601645>.
29. Syverud, K.; Kirsebom, H.; Hajizadeh, S.; Chinga-Carrasco, G. *Nanoscale Res. Lett.* **2011**, *6*(1), 626. <https://doi.org/10.1186/1556-276X-6-626>.
30. Chen, J.; Yeh, J.; Chen, C. *J. Appl. Polym. Sci.* **2003**, *90*(6), 1662.
31. Sannino, A.; Pappadà, S.; Madaghiele, M.; Maffezzoli, A.; Ambrosio, L.; Nicolais, L. *Polymer.* **2005**, *46*(25), 11206. <https://doi.org/10.1016/j.polymer.2005.10.048>.
32. Hsiung, H.; Huang, H.; Wang, Y.; Wang, C.; Chen, J.; Chen, C. *J. Appl. Polym. Sci.* **2004**, *92*(80), 3886.
33. Wang, C. C.; Chen, C. C. *Appl. Catal. Gen.* **2005**, *293*(1–2), 171. <https://doi.org/10.1016/j.apcata.2005.07.007>.
34. Egal, M.; Budtova, T.; Navard, P. *Cellulose.* **2008**, *15*(3), 361. <https://doi.org/10.1007/s10570-007-9185-1>.
35. Yao, W. H.; Chen, J. C.; Hu, M. S.; Teng, M. Y.; Huang, P. H.; Lin, J. M.; Chen, C. C. *J. Appl. Polym. Sci.* **2005**, *97*(2), 595. <https://doi.org/10.1002/app.21282>.
36. Remadevi, R.; Gordon, S.; Wang, X.; Rajkhowa, R. *Text Res. J.* **2017**, *88*, 1356. <https://doi.org/10.1177/0040517517700196>.
37. Gaspar, D.; Fernandes, S. N.; De Oliveira, A. G.; Fernandes, J. G.; Grey, P.; Pontes, R. V.; Pereira, L.; Martins, R.; Godinho, M. H.; Fortunato, E. *Nanotechnology.* **2014**, *25*(9), 094008. <https://doi.org/10.1088/0957-4484/25/9/094008>.
38. Kumar, S.; Rai, A. K.; Singh, V. B.; Rai, S. B. *Spectrochim. Acta, Part A: Mol. Biomol. Spectrosc.* **2005**, *61*(11–12), 2741. <https://doi.org/10.1016/j.saa.2004.09.029>.

39. Schenzel, K.; Fischer, S. *Cellulose*. **2001**, *8*(1), 49. <https://doi.org/10.1023/A:1016616920539>.
40. Wiley, J. H.; Atalla, R. H. *Carbohydr. Res.* **1987**, *226*, 113.
41. Maitra, J.; Shukla, V. K. *Am. J. Polym. Sci.* **2014**, *4*(2), 25. <https://doi.org/10.5923/j.ajps.20140402.01>.
42. Akhtar, M. F.; Hanif, M.; Ranjha, N. M. *Saudi Pharm J.* **2016**, *24*(5), 554. <https://doi.org/10.1016/j.jsps.2015.03.022>.
43. Kyle, S.; Jessop, Z. M.; Al-Sabaha, A.; Hawkins, K.; Lewis, A.; Maffei, T.; Charbonneau, C.; Gazzec, A.; Francis, L. W.; Iakovlev, M.; Nelson, K.; Eichhorn, S. J.; Whitaker, I. S. *Carbohydr. Polym.* **2018**, *198*, 270. <https://doi.org/10.1016/j.carbpol.2018.06.091>.
44. Tulonen, J.; Kolseth, F. *Holzforschung*. **1987**, *41*(4), 225.
45. Anseth, K. S.; Bowman, C. N.; Brannon-peppas, L. *Biomaterials*. **1996**, *17*(17), 1647.
46. Szcześniak, L.; Rachocki, A.; Tritt-Goc, J. *Cellulose*. **2008**, *15*(3), 445. <https://doi.org/10.1007/s10570-007-9192-2>.
47. Shirahashi, Y.; Watanabe, H.; Hayase, F. *Biosci., Biotechnol., and Biochem.* **2009**, *73*(10), 2287. <https://doi.org/10.1271/bbb.90382>.